

# UNDERSTANDING THE CRRT MACHINE

Helen Dickie

Renal Sister

Critical Care Unit

Guy's and St.Thomas' NHS Foundation Trust

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# RRT options - IHD vs CRRT (1)

|  | <b>PROS</b>  | <b>CONS</b>  |
|--|--|--|
| <b>Intermittent HaemoDialysis</b><br>e.g. 4hrs daily or on alternate days using on-line dialysis fluid | <ul style="list-style-type: none"><li>■ Less labour-intensive</li><li>■ Cheaper fluid (on-line supply)</li><li>■ Fewer machines needed</li><li>■ Dialysis fluid tailored to patient's needs</li><li>■ Shorter periods of anticoagulation</li><li>■ Allows patient to mobilise between treatment sessions</li></ul> | <ul style="list-style-type: none"><li>■ Fast fluid removal may not be well tolerated -&gt; intradialytic hypotension</li><li>■ May not be able to give optimal nutrition due to volume restriction</li><li>■ Usually operated by specialised dialysis nurses, not ICU staff</li><li>■ Water plant installation-expensive</li><li>■ Uses 1 circuit/day</li><li>■ Some blood loss each day</li></ul> |

# RRT options - IHD vs CRRT (2)

|  | <b>PROS</b>  | <b>CONS</b>  |
|--|--|--|
| <b>Continuous Renal Replacement Therapy</b><br>24h/24h if no interruptions due to circuits clotting or off-unit procedures | <ul style="list-style-type: none"><li>■ Fluid removed gradually – easier to remove large volumes of fluid</li><li>■ No restrictions on fluid input so full nutrition always possible</li><li>■ ICU staff operate the machines</li><li>■ Use of bagged fluid makes it possible to use machines anywhere</li><li>■ 1 circuit may last several days</li></ul> | <ul style="list-style-type: none"><li>■ More labour-intensive</li><li>■ Need 1 machine /patient</li><li>■ Uses bagged fluid - more expensive than on-line supply</li><li>■ No choice of fluid composition ('one size fits all')</li><li>■ Long periods of anticoagulation usually required</li><li>■ Patient 'tied' to machine – difficult to mobilise</li></ul> |

# RRT options – hybrid therapies

|  | <b>PROS</b>  | <b>CONS</b>   |
|--|--|---|
| <p><b>SLE(D)D</b><br/>= <b>Slow Extended (Daily) Dialysis</b><br/>or<br/><b>Sustained Low Efficiency (Daily) Dialysis</b><br/>= IHD run at slower rate for 8-12h daily or on alternate days</p> <hr/> <p><b>'Intermittent CRRT'</b><br/>= CRRT run at higher rate for 8-12h daily or on alternate days</p> | <ul style="list-style-type: none"><li>■ Fluid removed more gradually than in IHD so easier to remove large volumes of fluid without hypotension</li></ul> <hr/> <ul style="list-style-type: none"><li>■ Allows easier patient mobilisation than CRRT</li><li>■ Less labour-intensive than CRRT</li></ul> | <ul style="list-style-type: none"><li>■ May still not be as good as 24h/24h CRRT if pt. cardiovascularly unstable</li></ul> <hr/> <ul style="list-style-type: none"><li>■ Patient needs to be sufficiently stable</li><li>■ Uses 1 circuit/day</li><li>■ Some blood loss each day</li></ul> |

# CRRT machines

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Fresenius Multifiltrate

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Fresenius Multifiltrate



Gambro Prismaflex

# CRRT machines



Fresenius Multifiltrate



Gambro Prismaflex

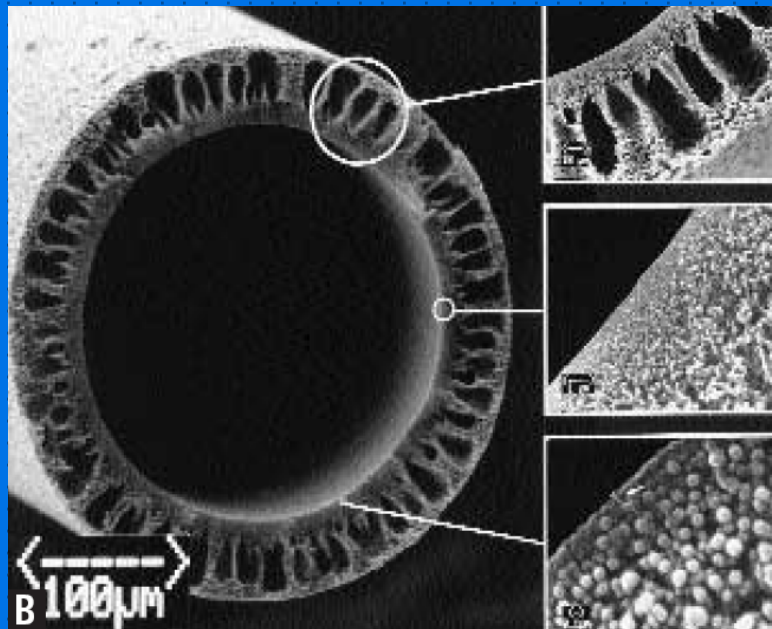


Nikkiso Aquarius

# Structure of haemofilter/dialyser

Bundle of hollow fibres, made of biocompatible synthetic material, in clear plastic cylinder.

Fibre material is semi-permeable, allowing water and molecules up to  $\sim 30,000$  Daltons to pass, but not the larger molecules and blood components, e.g. plasma proteins and blood cells



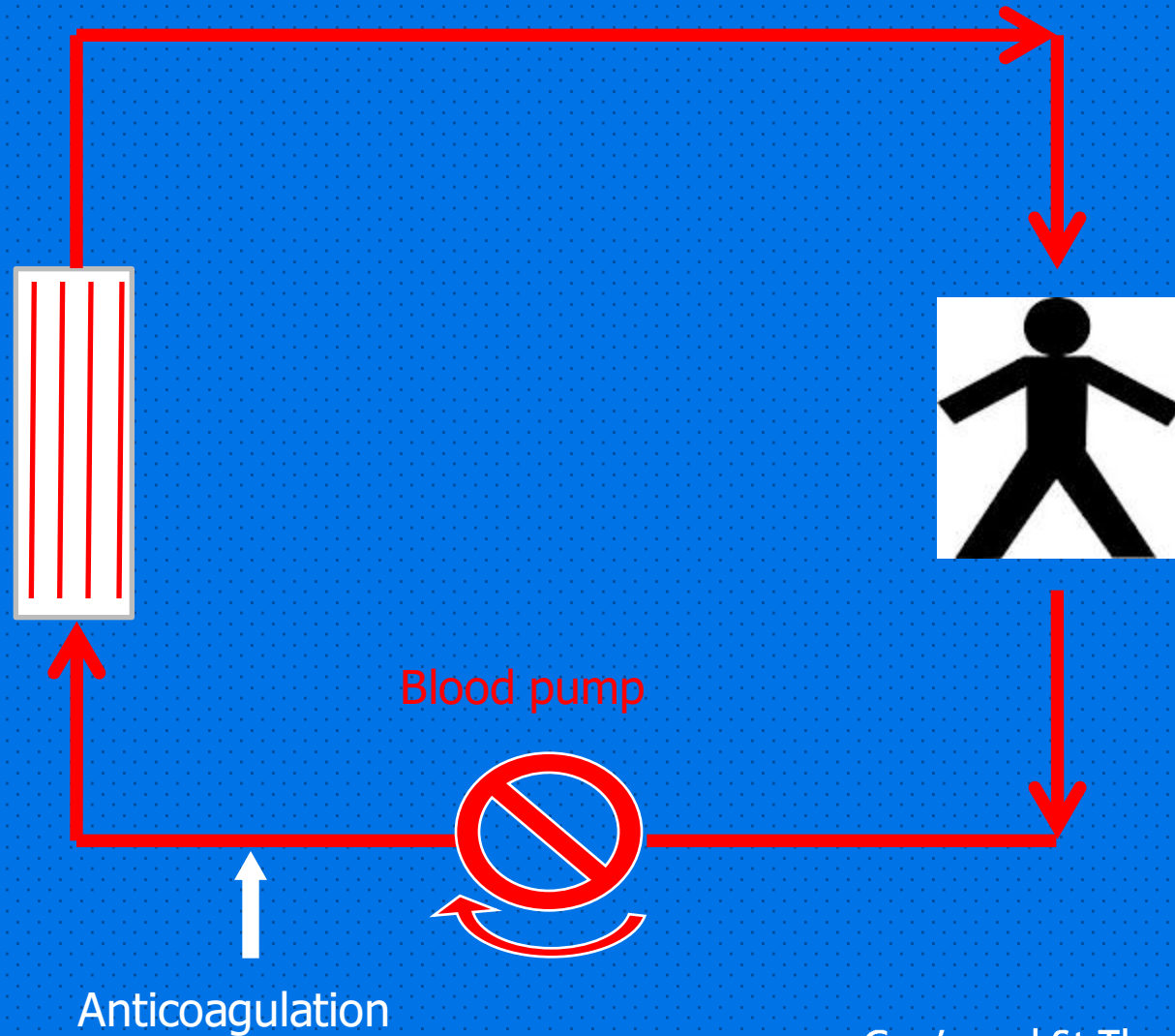
Internal diameter  $\sim 200\mu\text{m}$   
c.f.  $8\mu\text{m}$  for a capillary

# Possible modes of CRRT

- **SCUF** - Slow continuous Ultrafiltration
- **CVVH** -Continuous Veno-Venous Haemofiltration
- **CVVHD** - Continuous Veno-Venous Haemodialysis
- **CVVHDF** - Continuous Veno-Venous Haemodiafiltration

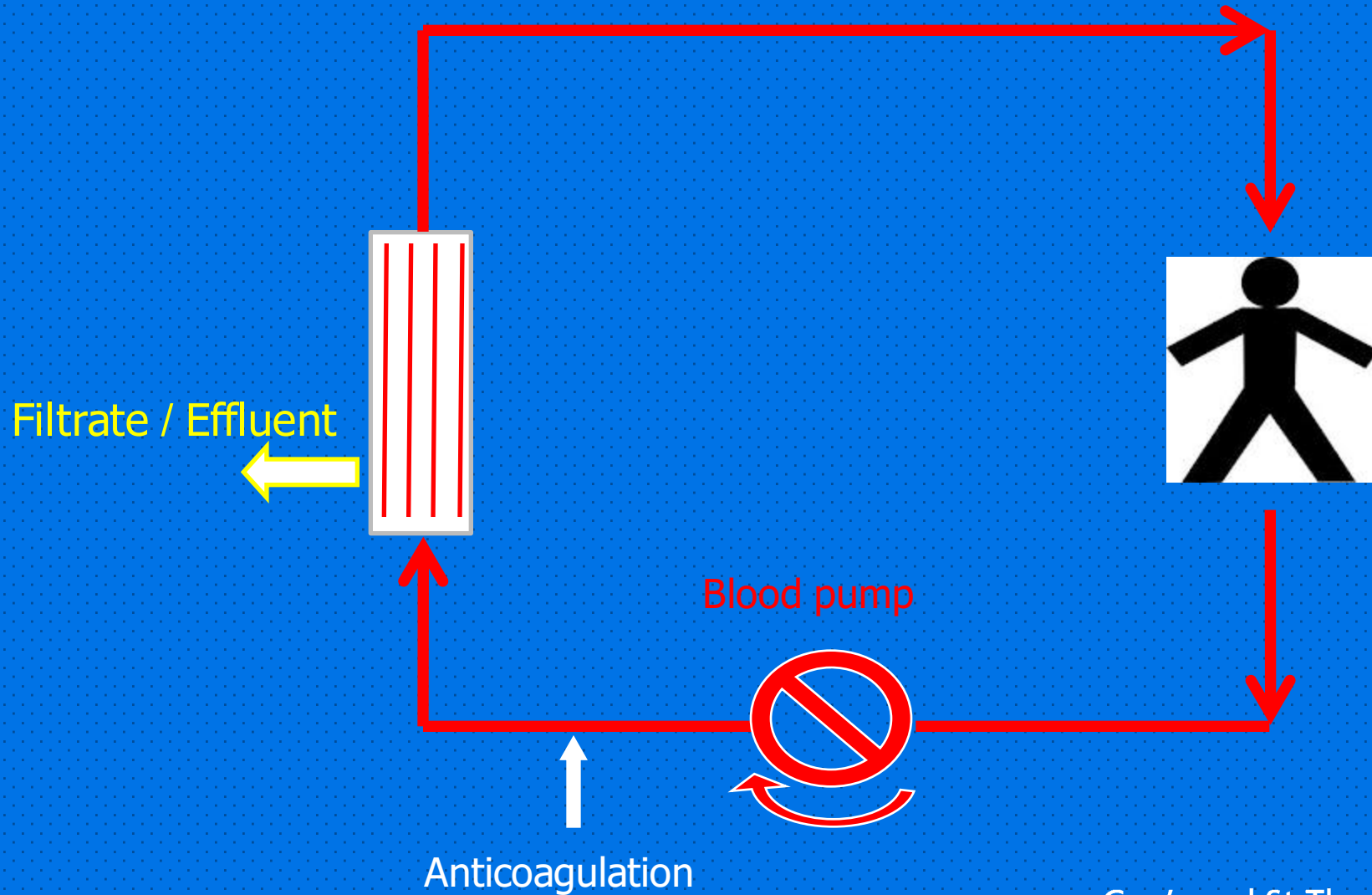
# Haemofiltration - 1

## the circuit



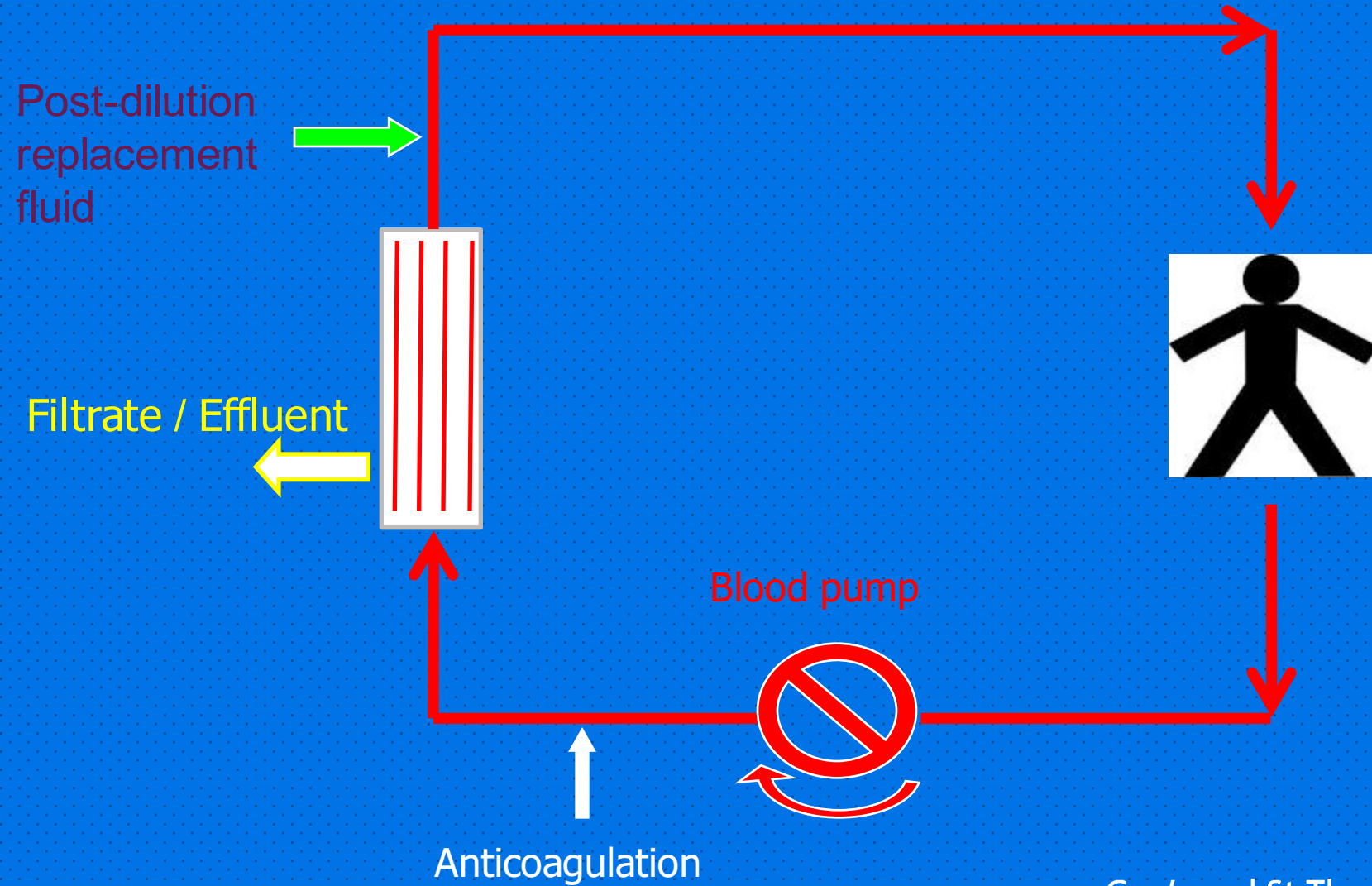
# Haemofiltration - 1

## the circuit



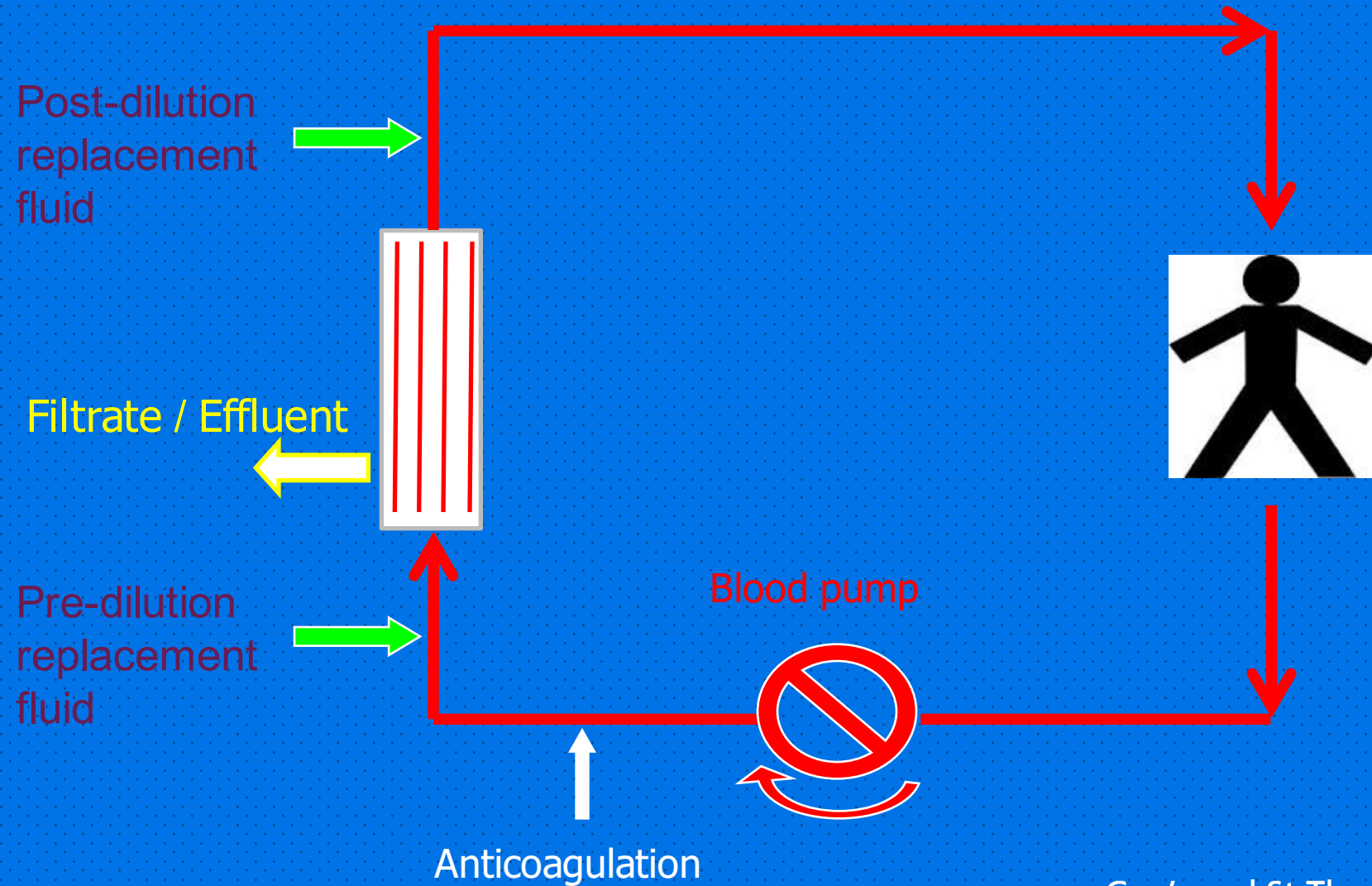
# Haemofiltration - 1

## the circuit



# Haemofiltration - 1

## the circuit



# Haemofiltration - 2

## Ultrafiltration with Convective solute clearance

- Water removed from the blood due to hydrostatic pressure difference
- Solutes carried over with the water by convection
- High volumes of ultrafiltrate are required to ensure adequate clearance of waste products of metabolism
- Loss of large volumes of ultrafiltrate from the blood requires simultaneous and continuous fluid replacement (substitution).  
If net loss is required, this replacement volume is less than the ultrafiltrate volume.

# Haemofiltration - 3

- Solute clearance depends on :
  - ultrafiltration flow rate
  - sieving coefficient of the solute in question
  - concentration of the solute in the plasma water (serum)
  - concentration of the solute in the replacement fluid
- Filtration rate = Net fluid loss rate + Replacement fluid rate
- Solute clearance can be achieved independently of changes in total body water.

# Haemofiltration - 4

**Pre-dilution** = replacement fluid enters blood circuit *before* the filter

**Post-dilution** = replacement fluid enters blood circuit *after* the filter

## Advantages of pre-dilution

- Does not cause haemoconcentration
  - ⇒ Reduced chance of clotting
- Reduced build-up of protein layer at blood-membrane interface
  - ⇒ Increased membrane efficiency

## Disadvantage of pre-dilution

- Ultrafiltrate is diluted
  - ⇒ decreased clearance of solutes

# Filtration Fraction (FF) - 1

- When plasma water removed by ultrafiltration, and only replaced after the filter (post-dilution), the blood becomes more viscous, or haemoconcentrated.
- Filtration Fraction refers to the fraction of plasma volume removed by ultrafiltration and is a measure of this haemoconcentration

# Filtration Fraction (FF) - 2

Correct formula:

$$\frac{\text{Post-dilution rate (L/h)} + \text{Net fluid loss (L/h)}}{\text{Blood flow rate (L/h)} \times (1 - \text{Hct})} \times 100 \%$$

Example :

Post-dilution rate 2000mL/h = 2.0L/h

Net fluid loss rate 100mL/h = 0.1L/h

Blood pump speed **200mL/min** = 1200mL/h = **12.0L/h**

Haematocrit 0.30

$$\text{FF} = \frac{2.0 + 0.1}{12.0 \times 0.70} \times 100\% = \frac{2.1}{8.4} \times 100\% = \mathbf{25.0\%}$$

# Filtration Fraction (FF) - 3

In practice **whole blood flow** is used to calculate FF:

$$\sim \frac{\text{Post-dilution rate (L/h)} + \text{Net fluid loss (L/h)}}{\text{Blood flow rate (L/h)}} \times 100 \%$$

Example 1:

Post-dilution rate 2000mL/h = 2.0L/h

Net fluid loss rate 100mL/h = 0.1L/h

Blood pump speed **200mL/min** = 1200mL/h = **12.0L/h**

$$\text{FF} = \frac{2.0 + 0.1}{12.0} \times 100\% = \frac{2.1}{12.0} \times 100\% = \mathbf{17.5\%}$$

# Filtration Fraction (FF) - 4

Increasing blood flow reduces FF:

$$\sim \frac{\text{Post-dilution rate (L/h)} + \text{Net fluid loss (L/h)}}{\text{Blood flow rate (L/h)}} \times 100 \%$$

Example 2:

Post-dilution rate 2000mL/h = 2.0L/h

Net fluid loss rate 100mL/h = 0.1L/h

Blood pump speed **300mL/min** = 1800mL/h = **18.0L/h**

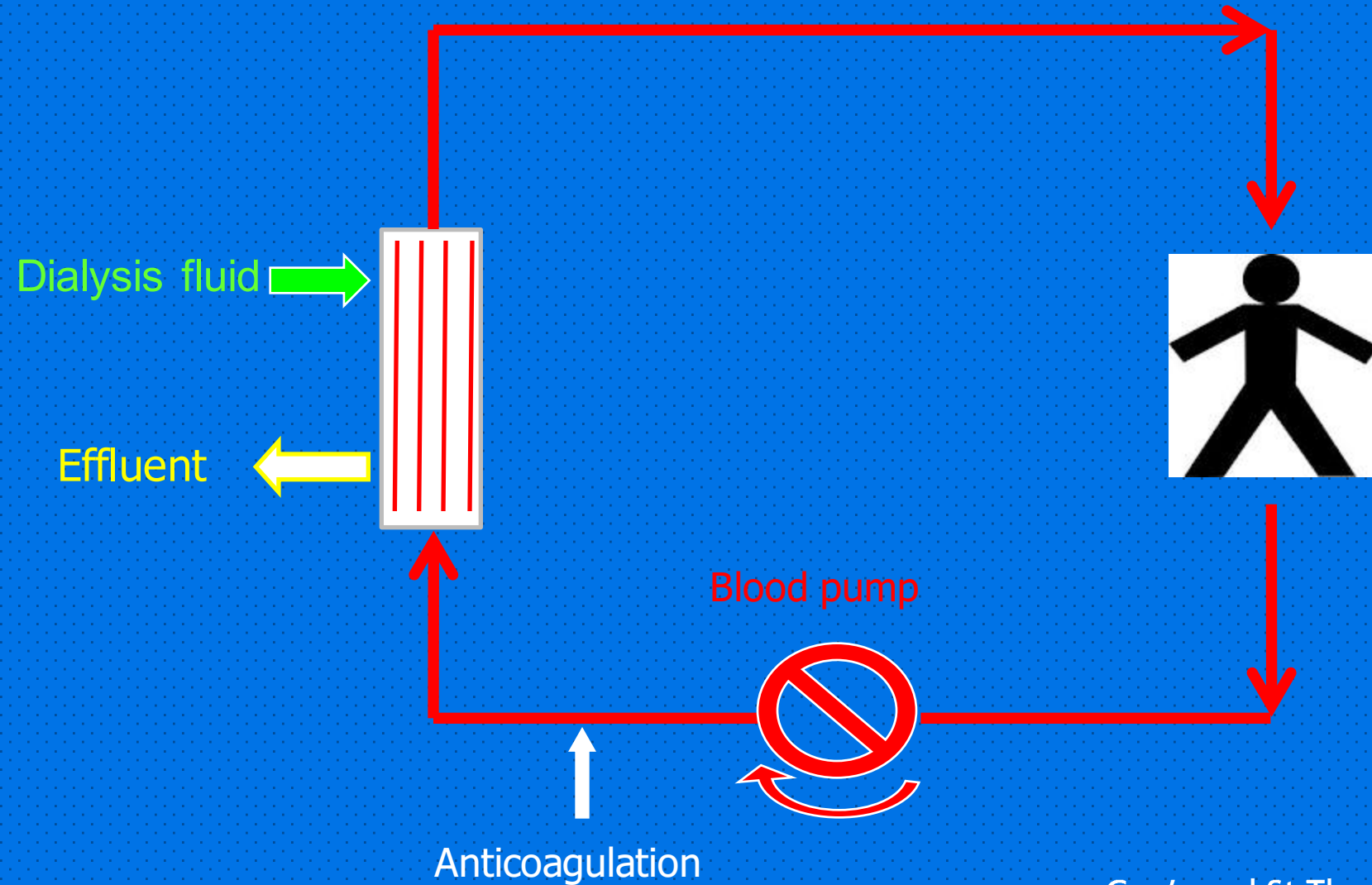
$$\text{FR} = \frac{2.0 + 0.1}{18.0} \times 100\% = \frac{2.1}{18.0} \times 100\% = \mathbf{11.7\%}$$

# Filtration Fraction (FF) - 5

- The higher the FF, the more haemoconcentrated the blood
- $\uparrow$  haemoconcentration  $\rightarrow$   $\uparrow$  tendency to clot
- Risk of filter clotting reduced by keeping FF  $< 20\%$
- Pre-dilution does not contribute to haemoconcn, so pre-dilution rate does not affect FF
- In dialysis, only net fluid loss causes haemoconcn.

# Haemodialysis - 1

## the circuit



# Haemodialysis - 2

- Based on principle of DIFFUSION of solutes across the membrane due to a concentration gradient.
- Dialysis fluid runs through the filter (dialyser) counter-current to the blood, which is flowing through the hollow fibres
- The semi-permeable hollow fibres allow the diffusion of solutes from the blood to the dialysis fluid if the concentration there is less than in the blood
- The greater this concentration gradient between the blood and the dialysis fluid, the greater the clearance

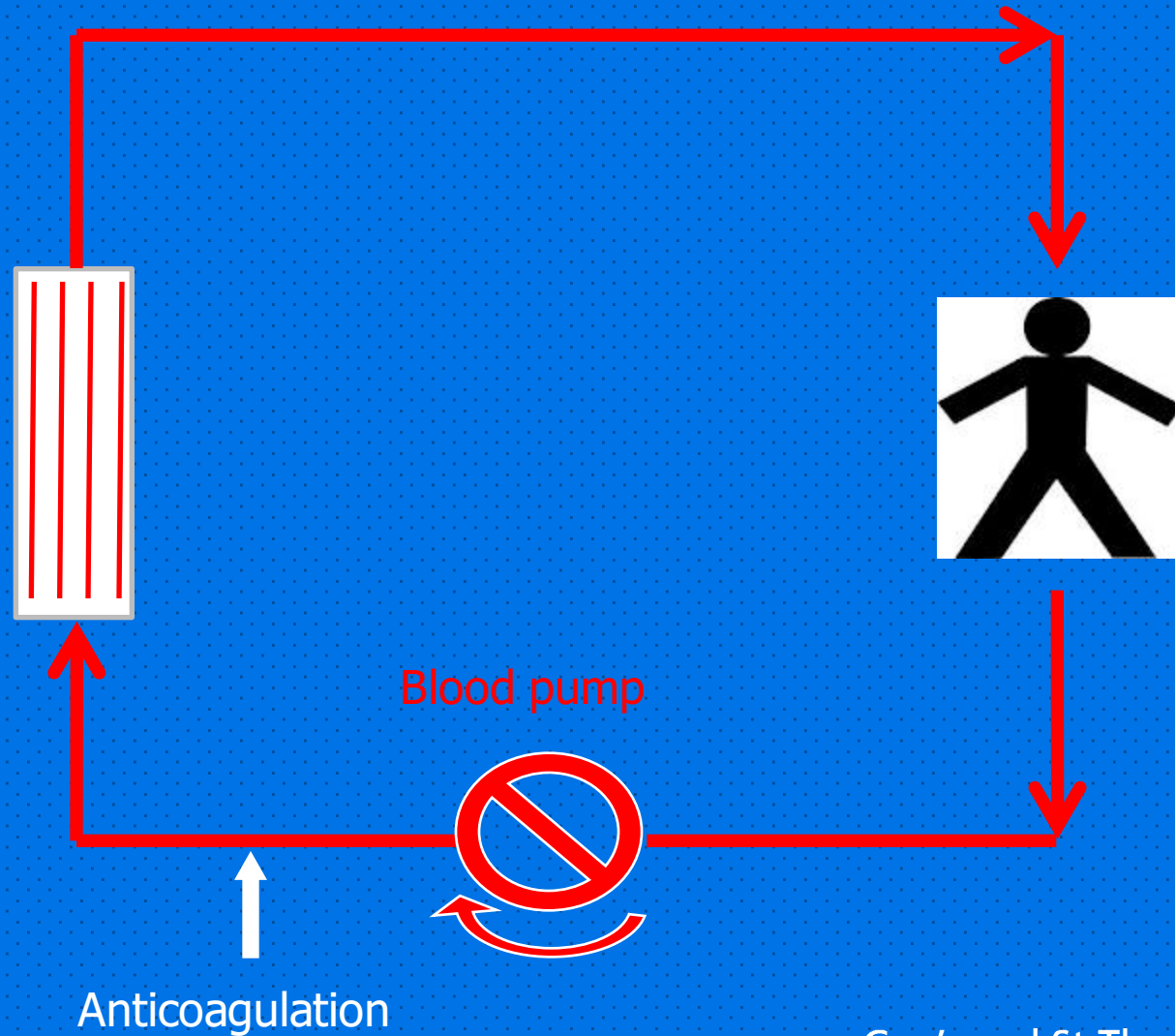
# Haemodialysis - 3

- Solute clearance depends on :
  - concentration of the solute in the dialysis fluid
  - concentration of the solute in the plasma water (serum)
  - dialysis fluid flow rate
  - blood flow rate
  - surface area of the filter (dialyser)
  - size of solute (smaller solutes cleared better)
- For water removal:
  - effluent pump runs at a higher rate than dialysate pump, so pulling the programmed amt. of water (net loss) from the blood through the semi-permeable membrane by ultrafiltration
  - Effluent rate = Net fluid loss rate + Dialysis rate
- Solute clearance can be achieved independently of changes in total body water.



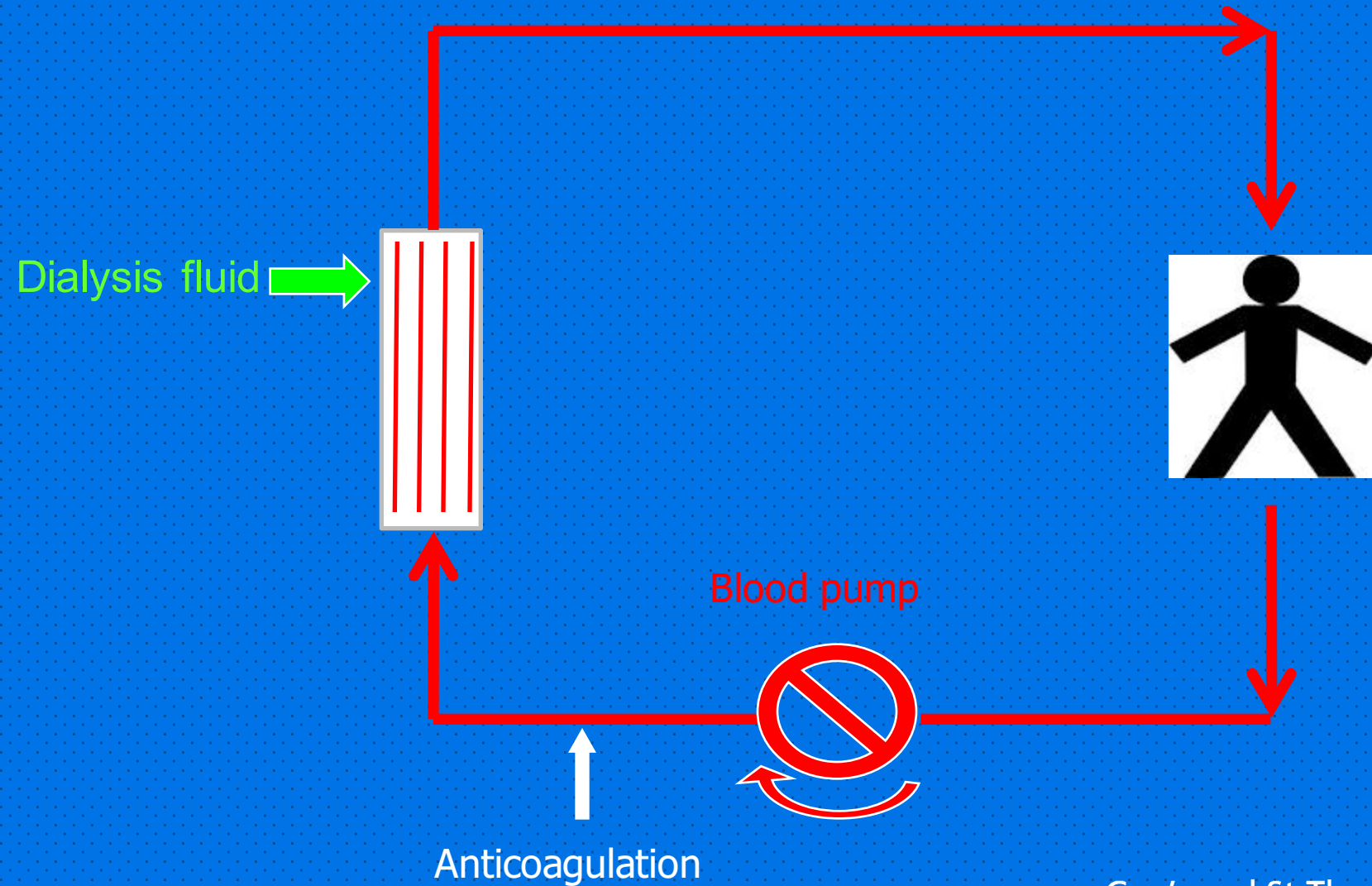
# Haemodiafiltration – 1

## the circuit



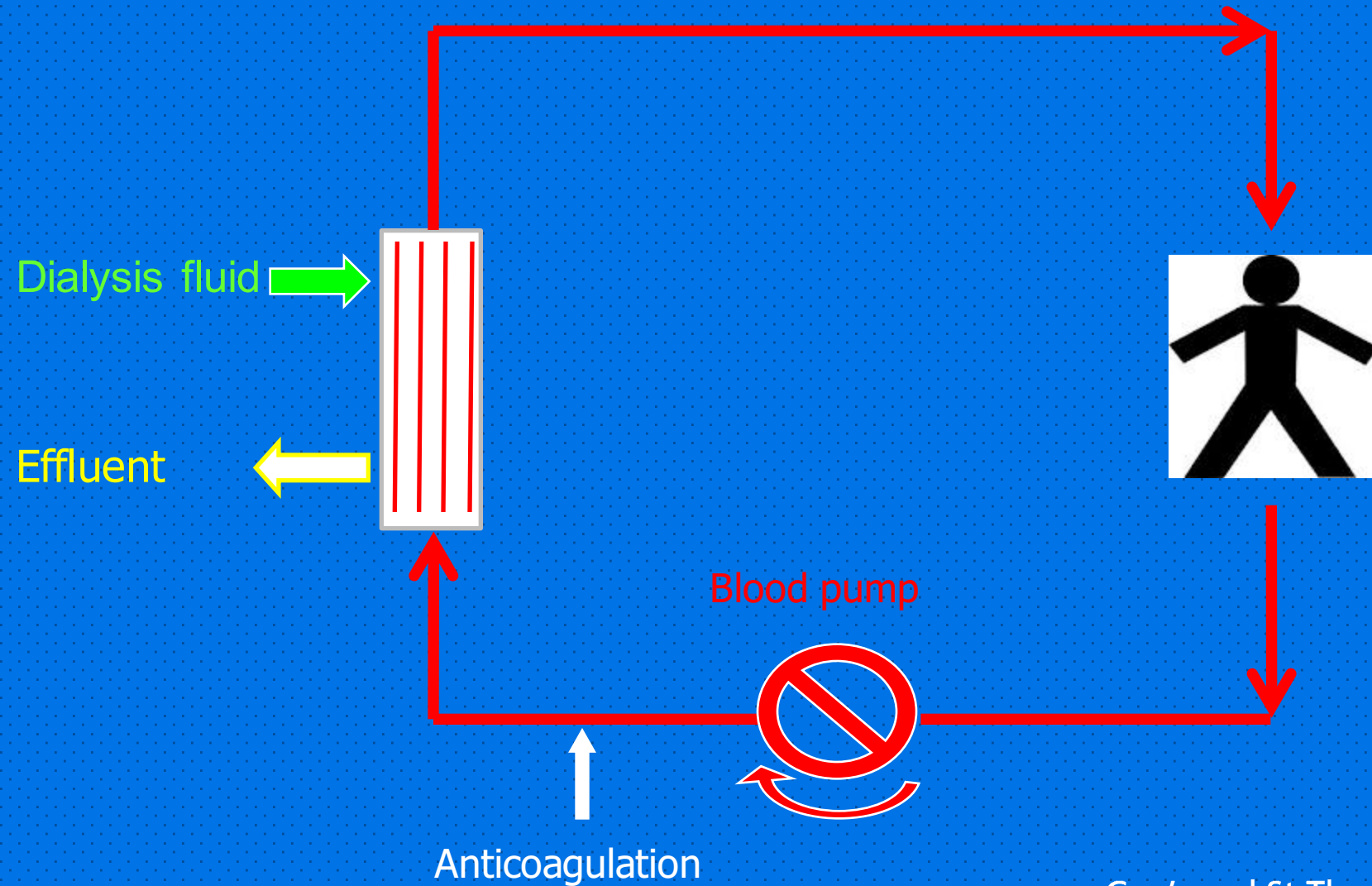
# Haemodiafiltration – 1

## the circuit

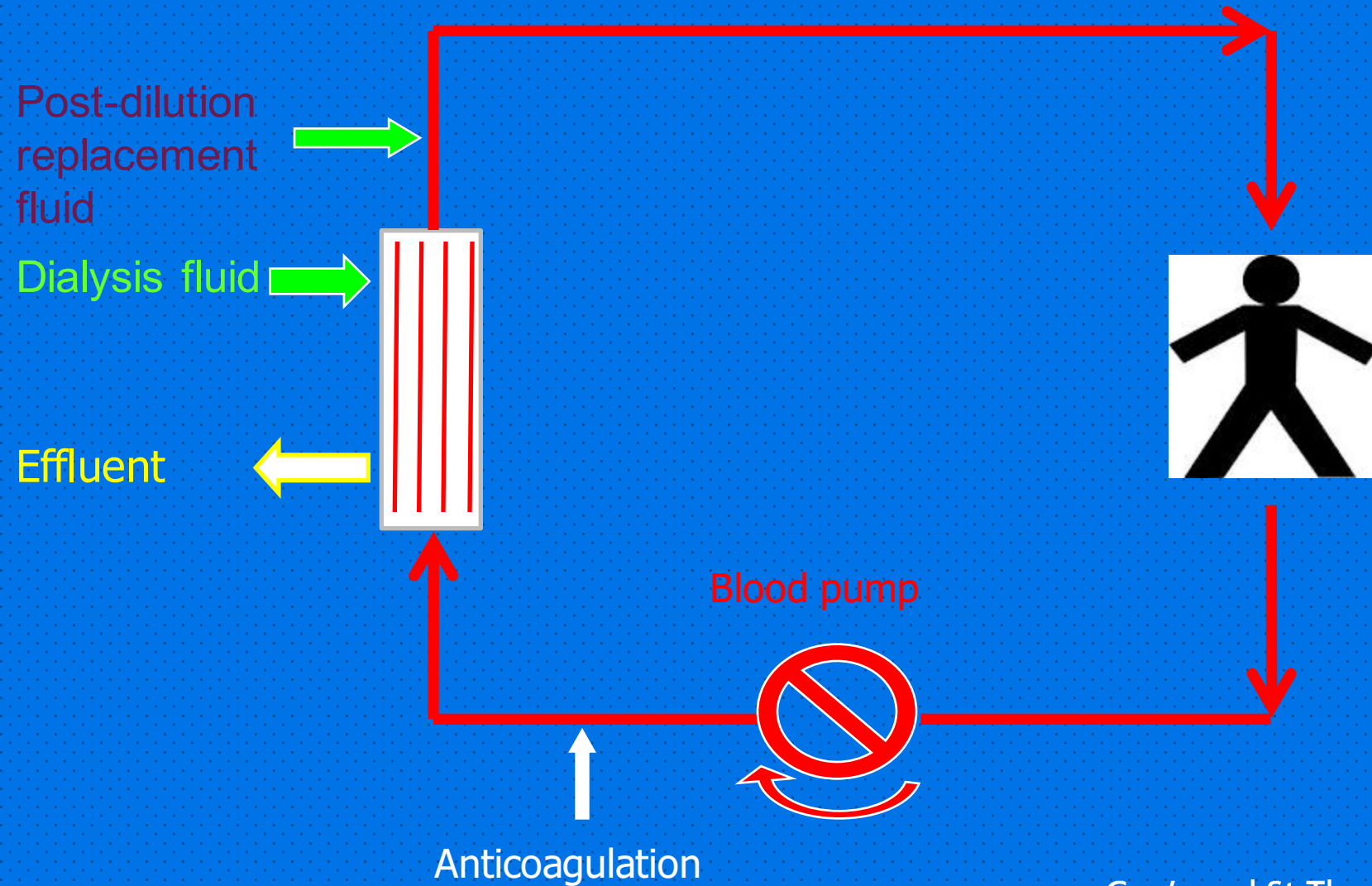


# Haemodiafiltration – 1

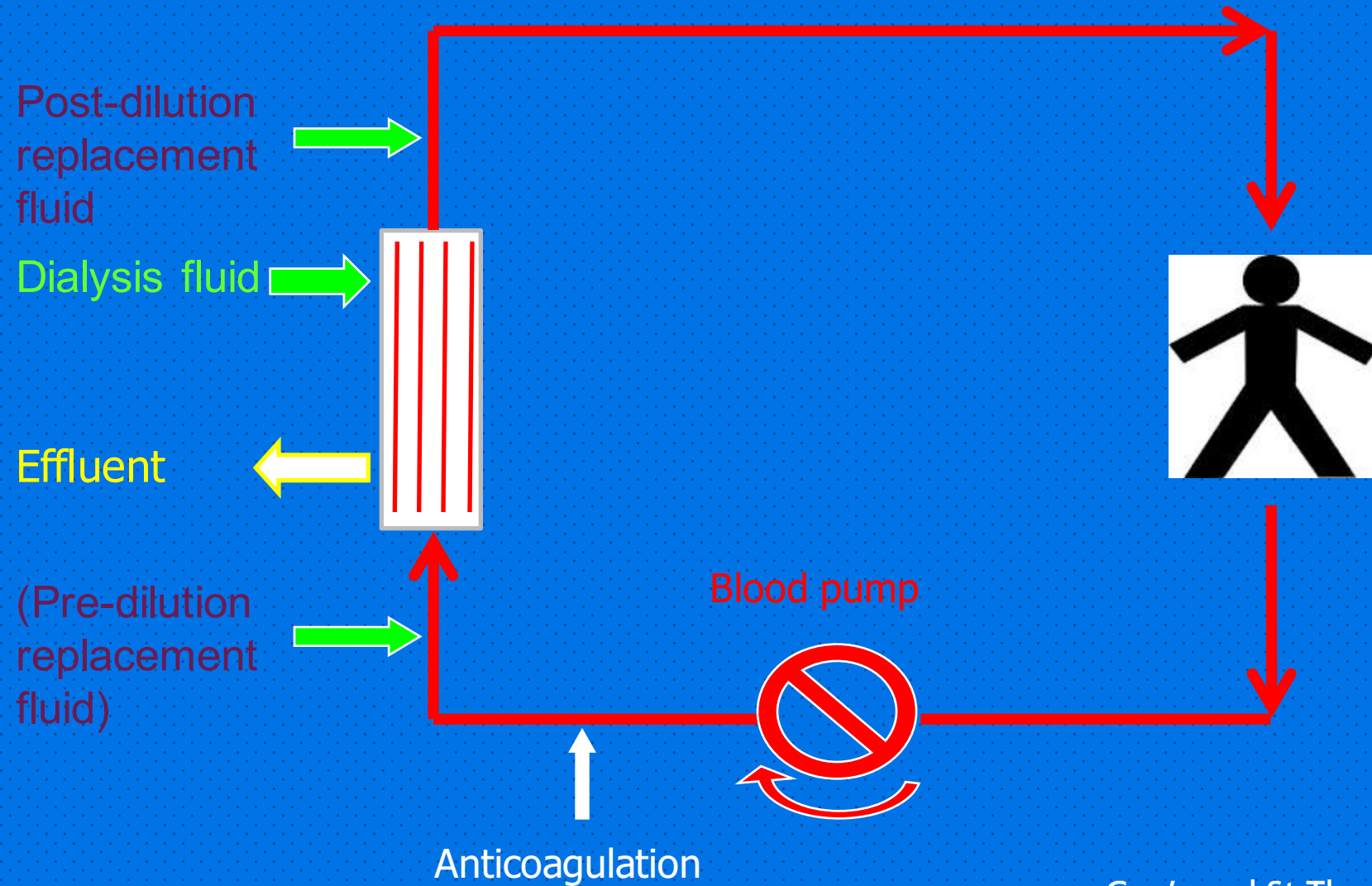
## the circuit



# Haemodiafiltration – 1 the circuit



# Haemodiafiltration – 1 the circuit



# Haemodiafiltration - 2

- Both diffusion and ultrafiltration+convection are used.
- Diffusion takes place from the patient's blood to the dialysis fluid, which runs countercurrent to the blood flow.
- HF occurs simultaneously, so replacement fluid must be given to the patient to compensate for the volume of ultrafiltrate removed less the volume of net loss desired.

# Dialysis / Replacement Fluid

- The same fluid is used, whether RRT method is HF, HD or HDF.
- The fluid contains physiological levels of sodium, calcium, magnesium, glucose and a buffer (usually bicarbonate). It may also contain phosphate.
- The concentration of potassium used depends on the patient's serum potassium level.

# Typical composition of a bicarbonate-buffered dial/repl fluid

Composition once the 2 compartments mixed :

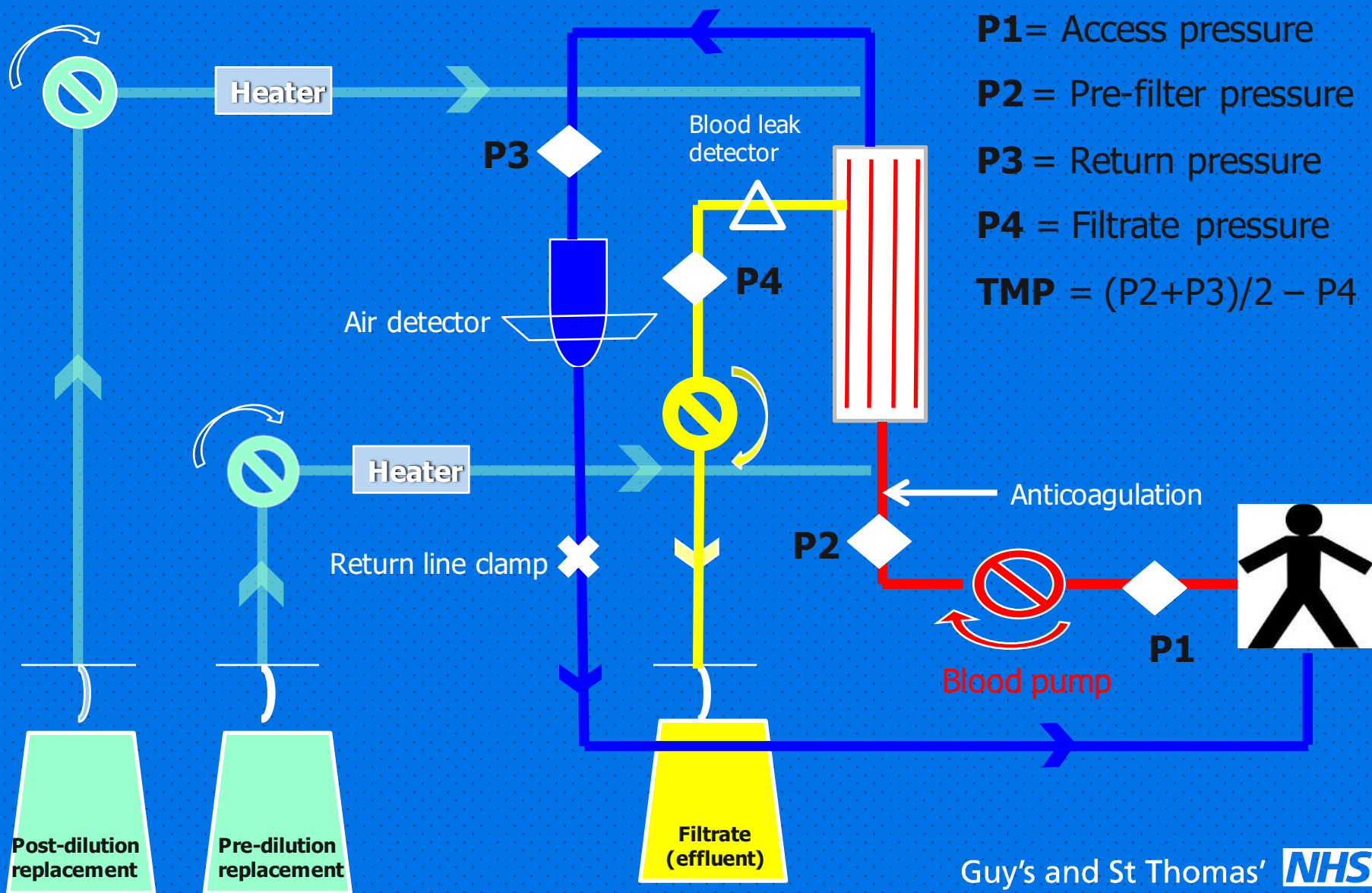
- $\text{Na}^+$  140 mmol/L
- $\text{K}^+$  **0, 2.0** or **4.0** mmol/L
- $\text{Ca}^{2+}$  1.5 mmol/L
- $\text{Mg}^{2+}$  0.5 mmol/L
- $\text{Cl}^-$  113 mmol/L
- $\text{HCO}_3^-$  35 mmol/L
- Glucose 5.55 mmol/L (1g/L)
- (Phosphate 1 mmol/L)

pH 7.4      Total Volume 5L

# Safety features of CRRT machines

- Bubble trap, air detector & return line clamp
- (Degassing chamber)
- Blood leak detector
- Pressure monitoring
- Scales sensitive to 1g weight change – Machine constantly monitors that rates of weight loss from treatment fluid bags and weight gain in effluent bags match the rates programmed
- Heating system for treatment fluids or blood lines

# Main features of CRRT circuit (CVVH)



**P1** = Access pressure  
**P2** = Pre-filter pressure  
**P3** = Return pressure  
**P4** = Filtrate pressure  
**TMP** =  $(P2 + P3) / 2 - P4$

# Blood Pump speed

- Aim for at least 200mL/min (12L/h) for non-citrate anticoagulation
- Higher PBS required for high filtration rates to avoid haemoconcentration /reduced clearance effects
- Higher PBS can increase clearance in dialysis
- Faster blood flow tends to reduce risk of clotting

Need optimal vascular access to  
achieve good blood flow

# RRT Rate and Dose

Total RRT Rate (mL/h) =

RRT Dose (mL/kg/h) x Body Weight (kg)

Pre-dilution replacement rate

Post-dilution replacement rate

Dialysis rate



Total RRT rate

# Circuit pressures

## Access pressure

- is negative in a venovenous circuit
- more negative if
  - increased resistance to blood flow into the circuit
  - increased blood pump speed

## Return and Pre-filter pressures

- are positive
- more positive if
  - increased resistance to post-blood pump flow
  - increased blood pump speed

# Circuit pressures

## Transmembrane pressure (TMP)

$$= \frac{(\text{Pre-filter pressure} + \text{Return pressure})}{2} - \text{Filtrate pressure}$$

i.e. pressure difference across the membrane

- is usually zero or positive
- more positive if
  - high rate of filtration (so TMP always much higher in CVVH than in CVVHD)
  - membrane pores are clogged causing resistance to flow
  - if low flux filter used
  - the blood compartment pressure is high

# Circuit pressure alarms

## Access pressure

Limit usually set at  $\sim - 300\text{mmHg}$

Risk of damage to vein wall and haemolysis

## Return pressure

Limit usually set at  $\sim + 500\text{mmHg}$

Risk of pushing clot forward / circuit blood leaks

## Pre-filter pressure

Limit usually set at  $\sim + 500\text{mmHg}$

Risk of pushing clot forward / circuit blood leaks

## TMP

Limit usually set at  $\sim + 300\text{mmHg}$

Risk of membrane rupture  $\rightarrow$  blood loss into effluent

When these alarms are triggered, the blood pump and the treatment pumps stop  $\rightarrow$   $\uparrow$  risk of clotting &  $\downarrow$  solute clearance

# Circuit pressures

- If no alarms, the machine is removing fluid and delivering filtration/dialysis precisely as programmed
- Increasingly –ve access pressure or +ve pre-filter, return or TMP pressures indicate machine having difficulty running as programmed.  
(Patient movement will then cause pressures to hit their alarm limit more easily.)
- **Good access & effective anticoagulation is critical to RRT success !!**

# Staff training and responsibilities

- Understand principles of CRRT
- Set up & connect circuit correctly
- Program treatment (incl. fluid loss) appropriately
- Monitor patient's response  
(cardiovascular status, acid-base balance, electrolytes, urea / creatinine)
- Manage anticoagulation
- Troubleshoot - prompt & correct response to alarms
  - to facilitate smooth running → optimising circuit life & clearance
  - to avoid fluid balance errors
- Recognise when circuit is clotting & should be washed back
- Recognise access failure